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TITLE:

CIRCUIT ARRANGEMENT AND
METHOD FOR GENERATING AN X-
RAY TUBE VOLTAGE

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CIRCUIT ARRANGEMENT AND METHOD FOR GENERATING AN X-RAY
TUBE VOLTAGE

5 The invention relates to a circuit arrangement for
generating an x-ray tube voltage, having an inverse
rectifier circuit for generating a high-frequency
alternating voltage, having a high-voltage generator for
converting the high- frequency alternating voltage into a
10 high voltage for the x- ray tube, and having a voltage
controller, which on the basis of a deviation of an actual
x-ray tube voltage from a set- point x-ray tube voltage
generates a first controlling variable value for a
controlling variable for the inverse rectifier circuit,
15 for achieving an adaptation of the actual x-ray tube
voltage to the set-point x-ray tube voltage. One such
circuit arrangement is known from German Patent DE 29 43
816 C2.

20 The invention also relates to an x-ray generator
having such a circuit arrangement, an x-ray system having
such an x-ray generator, and a corresponding method for
generating an x-ray tube voltage.

25 To generate an x-ray tube voltage, modern x-ray
generators often have circuit arrangements of the typed
defined at the outset. Since a line frequency is first
rectified and then converted back into a high-frequency
alternating voltage that is finally transformed to a
30 desired voltage, such generators are also known as high-
frequency generators. The voltage controller serves to
regulate the high voltage at the x-ray tube as optimally
as possible in terms of time to a diagnostically required
value with a requisite precision.

35 Compared to conventional generators, in which the

high voltage is first transformed using the line frequency present, then rectified, and finally delivered to the x-ray tube, such a circuit arrangement has the advantage that in principle, it can be made virtually independent of changes to a line voltage and to a tube current by means of a relatively fast closed-loop current circuit. The tube voltage is therefore highly replicable and can be kept constant. Compared to so-called direct voltage generators, in which a high voltage, transformed at line frequency and rectified, is finely regulated with the aid of triodes, high-frequency generators have the advantage of a relatively small structural volume and lower production costs. These advantages are the reason for the preferred use of such circuit arrangements in modern x-ray generators.

In conventional circuit arrangements of the type defined at the outset problems arise from the fact that parameters of a controlled system including an inverse rectifier and the high-voltage circuit, depending on the selected operating point of the x-ray tube, cover a wide range of values, and that in particular the inverse rectifier's resonance characteristic is a highly nonlinear member of the closed-loop control circuit. Moreover, if damage to the power semiconductor is to be avoided, an oscillating current of the inverse rectifier must not exceed a predetermined maximum value. In a conventional single-step x-ray tube voltage closed-loop control circuit, a control speed of the circuit must therefore be set to be at least slow enough that the oscillating circuit current, even during running up to speed or when being turned on, does not exceed the maximum allowable value. As a result, a small-signal behavior of the closed-loop control circuit is also slowed down, resulting in a slower elimination of interference

variables than would intrinsically be possible. Moreover, with this kind of a single-step control, the oscillating current is limited only indirectly. Therefore if the inverse rectifier is redimensioned, the control parameters
5 of the controller must be adapted to suit the oscillating current. A simple voltage controller can thus meet the demands, even if only to an unsatisfactory extent.

It is therefore the object to create an alternative
10 to the known prior art that permits high-speed control without exceeding the maximum allowable oscillating current.

This object is attained by a circuit arrangement as
15 defined by claim 1 and by a method as defined by claim 9.

To that end, the circuit arrangement additionally has a measurement circuit for measuring an oscillating current, applied to one output of the inverse rectifier
20 circuit, of the high-frequency alternating voltage. By means of an oscillating current controller, a second controlling variable value for the aforementioned controlling variable of the inverse rectifier circuit is then generated on the basis of a deviation of an
25 ascertained actual oscillating current value from a predetermined maximum oscillating current value. The voltage controller and the oscillating current controller are then coupled in series to a switching device, which compares a first controlling variable value and a second
30 controlling variable value and forwards only the lesser of the two controlling variable values, as the resultant controlling variable value, to the inverse rectifier circuit.

35 A second controlling variable value is ascertained

separately by means of an oscillating current controller on the basis of the deviations of an actual oscillating current value from a predetermined maximum oscillating current value and compared with the first controlling variable value of the voltage controller, and only the lesser of the two controlling variable values is delivered to the inverse rectifier circuit. It is attained that in a normal situation, very fast control by the voltage controller is accomplished; and only in extreme cases, if a critical range for the oscillating current is attained, is the voltage controller relieved by the oscillating current controller. In other words, in this "relief control", as long as the voltage controller is functioning "normally" and provides only an oscillating current that is less than the maximum allowable oscillating current, the controlling variable of the voltage controller will be sent on to the controlled system. Only if the maximum allowable oscillating current is reached or exceeded, which will be the case for instance during running up to speed as a rule, does the oscillating current controller come into play and limit the oscillating current to its maximum allowable value.

The dependent claims contain various especially advantageous features and refinements of the invention.

Preferably, for at least one of the two controllers and especially preferably for both controllers, a PI controller (proportional-integral controller) is used. An integral portion of the applicable controller has an object of forcing a steady-state control error, that is a control error in a steady state, to zero. Thus a persistent control deviation is reliably avoided. The controllers preferably then comprise series-connected proportional parts and integral parts. The advantage over

a parallel PI controller structure is that now the controller parameters pertaining to an amplification and an adjustment or a readjustment time can be set separately from one another. Instead of a PI controller, a PID

5 controller can also be used.

In an especially preferred exemplary embodiment, an output of the switching device is connected to one input of the voltage controller and/or of the oscillating
10 current controller, for feeding back the resultant controlling variable value. The voltage controller and/or the oscillating current controller are embodied such that they forward the resultant controlling variable value, if the controlling variable value generated by the applicable
15 controller is not forwarded as the resultant controlling variable value.

To that end, the applicable controller compares the resultant controlling variable with its own controlling
20 variable value that is internally also fed back. As a result of this variant, additional transient events caused by abrupt changes or surges upon switchover between the two controllers are reliably prevented.

25 Preferably, the switching device is embodied such that it sends at least a predetermined minimum controlling variable value as the resultant controlling variable value onward to the inverse rectifier circuit. Moreover, preferably at most, a predetermined maximum controlling
30 variable value is sent onward, as the resultant controlling variable value, to the inverse rectifier circuit. Hence, the result controlling variable is actively limited to a range between the minimum value and the maximum value.

35

Since the controller parameters, being the controller amplification and the readjustment time, are as a rule dependent on the operating point, the voltage controller and/or the oscillating current controller preferably can each vary at least one parameter (i.e., controller parameter) of the applicable controller as a function of a set x-ray tube voltage and/or as a function of a set x-ray tube current. That parameter is then fed to corresponding inputs of the respective controller, and as a result the parameters of the applicable controllers are suitably set internally.

A circuit arrangement according to the invention can in principle be used to generate an x-ray tube voltage in any conventional x-ray generator, regardless of how the x-ray generator is constructed in terms of its further components, such as the various measuring instruments or the supply of heating current. The invention can also be employed largely independently of the concrete embodiment of the inverse rectifier circuit and of the high-voltage generator.

The invention will be described in further details below in terms of exemplary embodiments in conjunction with the drawings. From the described examples and drawings, still other advantages, characteristics and details of the invention will become apparent. Shown are:

Fig. 1a, a circuit diagram of a prior art circuit arrangement embodiment, with an inverse rectifier circuit and a high-voltage generator for generating a high voltage for an x-ray tube;

Fig. 1b, a block diagram of an embodiment of a closed-loop control circuit for the prior art circuit

arrangement shown in Fig. 1a;

Fig. 2, a block diagram of an embodiment of the closed-loop control circuit in a circuit arrangement according to the invention; and

Fig. 3, a more-detailed block diagram of an embodiment of the closed-loop control circuit of an especially advantageous variant of the circuit arrangement of the invention.

In Fig. 1a, typical components of an x-ray generator are shown; they represent the controlled system for the control of the x-ray tube voltage $U_{R\delta}$. These typical components include first an oscillating current inverse rectifier G_{si} coupled to a high-voltage generator G_{su} , which is in turn coupled to an x-ray tube 6.

The inverse rectifier circuit G_{si} has a plurality of power semiconductors 3, which are connected accordingly such that an intermediate circuit direct voltage V_z is converted into a high-frequency voltage. The inverse rectifier circuit G_{si} furthermore has a voltage frequency converter 2, which converts a voltage value $Y(t)$ into a triggering frequency f_a , with which the power semiconductors 3 of the inverse rectifier G_{si} are triggered. The input voltage thus forms the controlling variable $Y(t)$ of the controlled system.

The inverse rectifier circuit G_{si} here is an oscillating circuit inverse rectifier (inverter). However, still other inverse rectifier circuits can be used, such as a square-wave inverse rectifier or arbitrary series-connected or multi-resonance inverse rectifiers.

The high-voltage generator G_{su} comprises first a transformer 4 with a transmission factor \ddot{u} and second, a rectifier and smoothing device 5 connected downstream of the transformer. The x-ray tube voltage $U_{R\ddot{o}}$ present at the output of the rectifier circuit and smoothing device 5 is delivered to the x-ray tube 6.

Fig. 1b shows a block diagram of a closed-loop control circuit according to the prior art. The inverse rectifier circuit G_{si} is represented here as a function block that includes a proportional transmission factor K_{si} and a time constant T_{si} . In particular, the proportional transmission factor K_{si} , because of resonance phenomena in the inverse rectifier G_{si} , is highly nonlinear, or in other words depends on the operating point of the inverse rectifier G_{si} .

The high-voltage generator G_{su} is also shown as a function block. It can be described by the proportional transmission factor K_{su} and the time constant T_{su} ; both of these variables are directly dependent on the x-ray tube voltage $U_{R\ddot{o}}$ and the x-ray tube current $I_{R\ddot{o}}$, or in other words, as a function of the operating point, both of these variables cover a wide range of values. The oscillating current of the inverse rectifier G_{si} is represented by the symbol $i_{sw}(t)$ and supplies the primary winding of the high-voltage transformer 4 of the high-voltage generator G_{su} . To avoid damaging the power semiconductors 3 in the inverse rectifier circuit G_{si} , the oscillating current $i_{sw}(t)$ must not exceed a maximum value.

In the prior art, to regulate the output voltage of the high-voltage generator G_{su} , an actual voltage $V_U(t)$ applied there at a certain instant t is compared with a set-point value $W_U(t)$, which corresponds to the desired x-

ray tube voltage U_{R0} ; that is, the difference is delivered to a voltage controller G_{RU} , which is once again shown here in the form of a function block.

5 This voltage controller G_{RU} is conventionally a simple PI controller, which as a function of the deviation of the actual value $V_U(t)$ from the set-point value $W_U(t)$ generates the controlling variable $Y(t)$, which is then fed to the input of the voltage frequency converter 2 of the
10 inverse rectifier circuit G_{Si} .

 In this kind of conventional closed-loop control circuit shown in Fig. 1b, the control speed of the voltage controller G_{RU} must be adjusted or set so slowly that the
15 oscillating current $i_{sw}(t)$ does not exceed the maximum allowable value even during running up to speed. This means that a fast control is not possible with the voltage controller G_{RU} , and thus interference can also be eliminated only slowly. Upon a re-dimensioning of the
20 inverse rectifier circuit G_{Si} , the controller parameters of the voltage controller G_{RU} must also be adapted accordingly, only an indirect limitation of the oscillating current $i_{sw}(t)$ is accomplished.

25 Fig. 2, in comparison to Fig. 1b, clearly shows the change according to the invention in the structure of the closed-loop control circuit. In this relief control, a switchover 8 is made according to the invention between two closed-loop control circuit structures of
30 substantially parallel construction.

 As in the prior art of Fig. 1b, here as well the x-ray tube voltage controller G_{RU} suitably forms a controlling variable $Y_U(t)$ from the difference between the
35 desired x-ray tube voltage, that is, the set-point voltage

$W_U(t)$, and the factual x-ray tube voltage, that is, the actual x-ray tube voltage $V_U(t)$.

In addition, the oscillating current $i_{sw}(t)$ is
5 measured by means of a smoothing member 7. This smoothing member 7 is described in terms of control technology by the additional time constant T_{MI} . The actual oscillating current value $V_I(t)$ thus ascertained is compared with a maximum allowable oscillating current value W_{I_max} (or set-
10 point value); that is, the difference between these values is formed and delivered to a further controller, which is the oscillating current controller G_{RI} , which likewise forms a controlling variable value $Y_I(t)$ for the controlling variable for the inverse rectifier circuit G_{si} .

15

Both the first controlling variable value $Y_U(t)$, which is formed by the voltage controller G_{RU} , and the second controlling variable value $Y_I(t)$, which is formed by the oscillating current controller G_{RI} , are delivered to a
20 switching device 8. From between the two controlling variable values $Y_U(t)$ and $Y_I(t)$, this switching device 8 selects the controlling variable value $Y_U(t)$, or $Y_I(t)$ that at the current instant t is the lesser of the two, and sends the controlling variable value $Y_U(t)$, or $Y_I(t)$, as
25 the resultant controlling variable value $Y(t)$, onward to the inverse rectifier circuit G_{si} .

Here, both the controllers G_{RI} , G_{RU} include a PI controller. A persistent control deviation is avoided by
30 means of the integral component of the PI controller.

This relief control according to Fig. 2 has the advantage that in a "normal case", the voltage controller G_{RU} is responsible for regulating the x-ray tube voltage.
35 Only in those cases when the actual controlling variable

value $Y_U(t)$ generated by the voltage controller G_{RU} would cause the oscillating current $i_{sw}(t)$ to exceed an allowed maximum value is the actual controlling variable value $Y_I(t)$ generated by the oscillating current controller G_{RI} less than the controlling variable value $Y_U(t)$ generated by the voltage controller G_{RU} . In those cases, the voltage controller G_{RU} is therefore rendered quasi-inoperative, and only the oscillating current controller G_{RI} is active. This has the advantage that the voltage controller G_{RU} can be adjusted considerably faster than in a closed-loop control circuit according to the prior art, and interference variables can thus be eliminated correspondingly quickly. Nevertheless, the relief in extreme cases reliably prevents the oscillating current $i_{sw}(t)$ from exceeding the allowed maximum value.

Given the structure of the invention, in the normal case the x-ray tube voltage control itself is not slowed down by the measuring time constant T_{MI} of the oscillating current $i_{sw}(t)$, since the smoothing member 7 is not located in the closed-loop control circuit for the x-ray tube voltage.

Since the parameters of the two partial controlled systems are each dependent on the operating point of the x-ray tube 6, the dimensioning of the two controllers G_{RU} , G_{RI} can be facilitated substantially if their parameters, being the controller amplifications and the readjustment times, are controlled as a function of the operating point. To that end, as schematically shown in Fig. 2, the values for the set x-ray tube voltage U_{R0} and the set x-ray tube current I_{R0} are delivered to the two controllers G_{RI} , G_{RU} , respectively.

Fig. 3 shows a more-detailed structural view of the

closed-loop control circuit of Fig. 2; here the closed-loop control circuits have additional, especially advantageous characteristics.

One additional characteristic is that the switching device 8 here has still further inputs, by way of which a maximum controlling variable value Y_{\max} and a minimum controlling variable value Y_{\min} are specified to the switching device 8. The switching device 8 is constructed such that at least the minimum controlling variable value Y_{\min} and at maximum the maximum controlling variable value Y_{\max} are output. In other words, a controlling variable range is dynamically specified, within which the controlling variable $Y(t)$ sent onward at that time to the inverse rectifier circuit G_{Si} varies. The maximum controlling variable value Y_{\max} and the minimum controlling variable value Y_{\min} are as a rule set at the factory. To this extent, they can already be predetermined by means of the suitable design of the switching device 8 itself.

Fig. 3 also shows a further detailed structure of the voltage controller G_{RU} and of the oscillating current controller G_{RI} . These are both PI controllers, with a proportional component 12, 15 and an integral component 13, 14 series-connected with it. In terms of control technology, the proportional components 12, 15 are each determined by transmission factors K_{PRI} and K_{PRU} , respectively; and the integral components 13, 14 are determined by time constants T_{NI} and T_{NU} , respectively.

This construction shown in Fig. 3, with series-connected proportional components 12, 15 and integral components 13, 14 has an advantage, over a parallel PI controller structure, in that the controller amplifications K_{PRI} , K_{PRU} and the readjustment times T_{NI} , T_{NU}

can each be set separately from one another.

As a further characteristic in this exemplary embodiment, the resultant controlling variable value $Y(t)$ is fed back by a connection of the output 9 of the switching device 8 to additional inputs 10, 11 of the voltage controller G_{RU} and the oscillating current controller G_{RI} , respectively. Internally, the controlling variable value

$Y_U(t)$ or $Y_I(t)$, generated by the respective controller G_{RU} or G_{RI} and is fed back to upstream of the integral component 13 or 14, and the difference between the fed-back, resultant controlling variable value $Y(t)$ and each specific controlling variable value $Y_U(t)$, $Y_I(t)$ is formed.

This means that the two controllers G_{RU} , G_{RI} each have limitation observers, which are coupled such that the integral component 13, 14 of whichever controller G_{RU} , G_{RI} is inactive at the time is carried along with the integral component 13, 14 of the active controller - that is, the controller G_{RU} or G_{RI} whose controlling variable value $Y_U(t)$, $Y_I(t)$ just then forms the resultant controlling variable value $Y(t)$. In this way, interference upon switchover between the controllers G_{RU} , G_{RI} is avoided.

Otherwise, there would be the risk that the controllers G_{RU} , G_{RI} run up to a stop, which would cause the integral components 13, 14 to be overloaded. That in turn would worsen a transient response upon a switchover (known as a wind-up effect).

Once again, it will be pointed out that the circuit arrangements shown in the drawings are solely exemplary embodiments, and for one skilled in the art, many possible variations exist for achieving a circuit arrangement according to the invention. For instance, adaptive

control of the voltage controller can be done, in such a way that the readjustment time is set as a function of the actual value of the tube voltage over the course of the tube voltage.